

Modular dual mobility (MDM) hip systems: Is there a risk of fretting corrosion?

Discussion points

- Metal ions released as a result of fretting corrosion may cause adverse local tissue reactions (ALTR) that can lead to implant revision¹
- Implant retrieval has confirmed occurrence of fretting corrosion of the cobalt-chromium (CoCr) liner of MDM implants²⁻⁸
- Elevations in serum metal ions compared to reference levels from healthy volunteers have been detected in patients who received an MDM implant that utilises a CoCr liner^{1,9-11}
- Malseated liners may be at risk for fretting corrosion¹²

The need for MDM systems

Dual mobility (DM) acetabular components have been designed to deliver increased range of motion with good stability, whilst reducing wear, in primary and revision total hip arthroplasty (THA) compared to standard implant designs.^{1,13} However, use of monoblock DM systems can be limited by the absence of holes for supplemental screw fixation and the inability to attach an implant insertion handle to the acetabular shell.¹

To address this need, current MDM systems include a CoCr liner between the titanium shell and the polyethylene (PE) articulating insert (Figure 1). This allows for screw fixation while providing an optimal surface for movement of the PE insert.¹

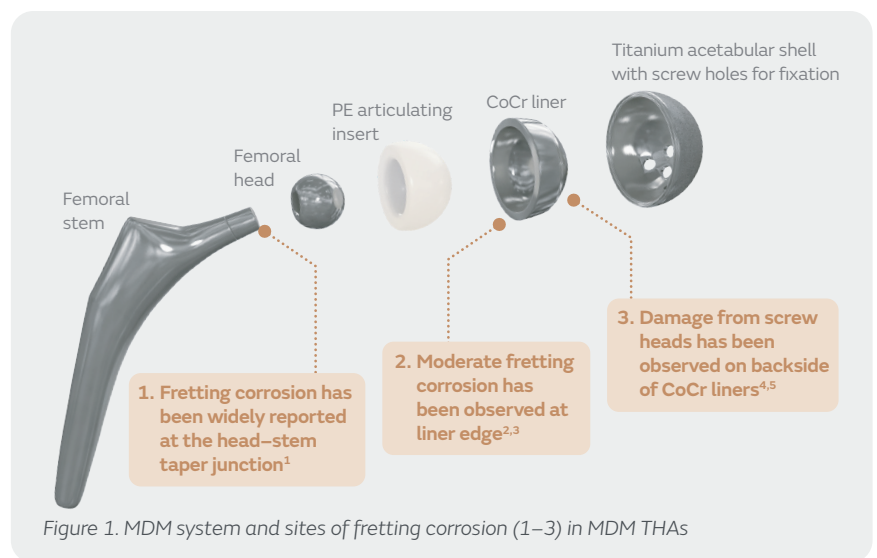


Figure 1. MDM system and sites of fretting corrosion (1-3) in MDM THAs

Is the liner-shell interface of MDM a risk for fretting corrosion?

Fretting corrosion is the damage caused by micromotion between two surfaces that results in the release of metal ions following exposure of non-oxidised metal to body fluids.¹⁴ This normally occurs at the modular junctions (trunnion) of the THAs (eg, femoral head-stem), with the release of metal ions, specifically cobalt (Co), potentially leading to ALTR and subsequent revision.¹ In MDM implants, the CoCr liner interfacing with the titanium shell creates an additional modular junction at which fretting corrosion could occur (Figure 1).¹⁻⁵

To help quantify this risk, a systematic literature review was performed to establish the current evidence base for fretting corrosion of the CoCr liner of MDM hip implants.¹⁵

The literature review identified 16 publications that examined fretting corrosion in MDM implants; 15 clinical studies and one *in vitro* study. Of these, 14 publications investigated MDM[®] systems manufactured by Stryker Orthopedic (Mahwah, NJ, USA), one used MDM implants from Lima Corporate Spa (Villanova di San Daniele del Friuli, Italy) and one did not specify the type of implant considered. Key findings from these studies are summarised in this report. An overview of the characteristics of the 15 clinical studies are presented in Table 2.

Throughout this review, 'MDM' refers to the generic design of the modular hip system. Where a reference is made specifically to the MDM model manufactured by Stryker, this has been referred to as 'MDM (Stryker)'.

*Performed using Embase and PubMed to identify all relevant studies that detailed the use of MDM hip systems and the incidence of fretting corrosion as of 13 May 2021. There was no restriction on publication date and no other search filters were applied. Further relevant articles were identified by pragmatic searching of Google Scholar (screening through the first 10 pages of hits) and review of internal Smith+Nephew evidence library. Exclusion criteria were the absence of relevant data on fretting corrosion, off-label usage, duplicate publications and publications with only the abstract available, including conference abstracts.¹⁵

+ Evidence in focus

How is fretting corrosion of the CoCr liner assessed?

1. MDM implant retrieval

Analysis of retrieved implant components provides the most reliable evidence of fretting corrosion of the CoCr liner (Figure 2).

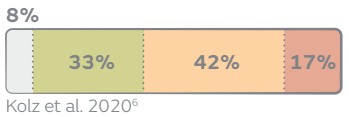
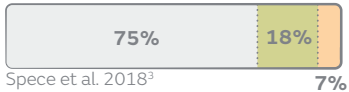
Retrieval studies are able to provide clear evidence of fretting corrosion, however, as implants are collected during revision surgeries, they may not describe the behaviour of well-functioning implants. The mean length of implantation with MDM implants across these studies is short- or mid-term. Fretting corrosion is a time-dependent phenomenon; therefore, longer implantation times may correlate to higher fretting corrosion scores. More data, however, are required to confirm this.

Of the identified studies...

5 reported fretting corrosion in **retrieved MDM implants**²⁻⁶

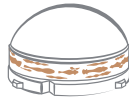
Two studies demonstrated fretting corrosion of varying severity in retrieved MDM (Stryker) implants from primary and revision THA.^{3,6}

None Mild Moderate Severe

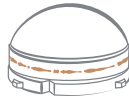


Three corrosion patterns were identified:⁶

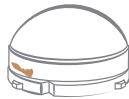
Generalised



A stripe about the middle of the taper region



Focal areas of the taper closest to the joint surface



In one study, fretting corrosion was shown to be more severe with MoM implants versus MDM (Stryker) implants, however, the former group had a higher LOI²

MoM 66±34

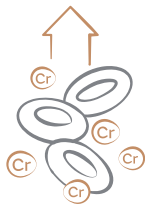
MDM 15±23

Mean±SD
p<0.01

Two studies noted fretting corrosion damage to the CoCr liner of MDM (Stryker) implants^{4,5}



In a study specifically investigating fretting corrosion at the taper junction, Lombardo et al. identified fretting corrosion at the screw-liner interface⁵



In a study investigating rTHA survivorship and dislocation rate, in one patient with elevated serum Cr; Sutter et al. found scuffing thought to be from screws⁴

2 case studies reported fretting corrosion in **CoCr liners**^{7,8}



Abdelaal et al. identified one patient requiring revision surgery due to IPD with moderate to/or severe corrosion of the liner eight years post surgery⁷



Sonn et al. identified three patients with fretting corrosion at the shell-liner interface, which in two cases was found to be canted⁸

Figure 2. Evidence of fretting corrosion of the CoCr liner from MDM implant retrieval studies

CoCr = cobalt-chromium, Cr = chromium, IPD = intraprosthetic dislocation, LOI = length of implantation, MDM= modular dual mobility, MoM = metal-on-metal, rTHA = revision total hip arthroplasty, THA = total hip arthroplasty

+ Evidence in focus

2. Serum metal ions

The literature review included ten publications that detailed metal ion levels in patients who received MDM implants (Figure 3).

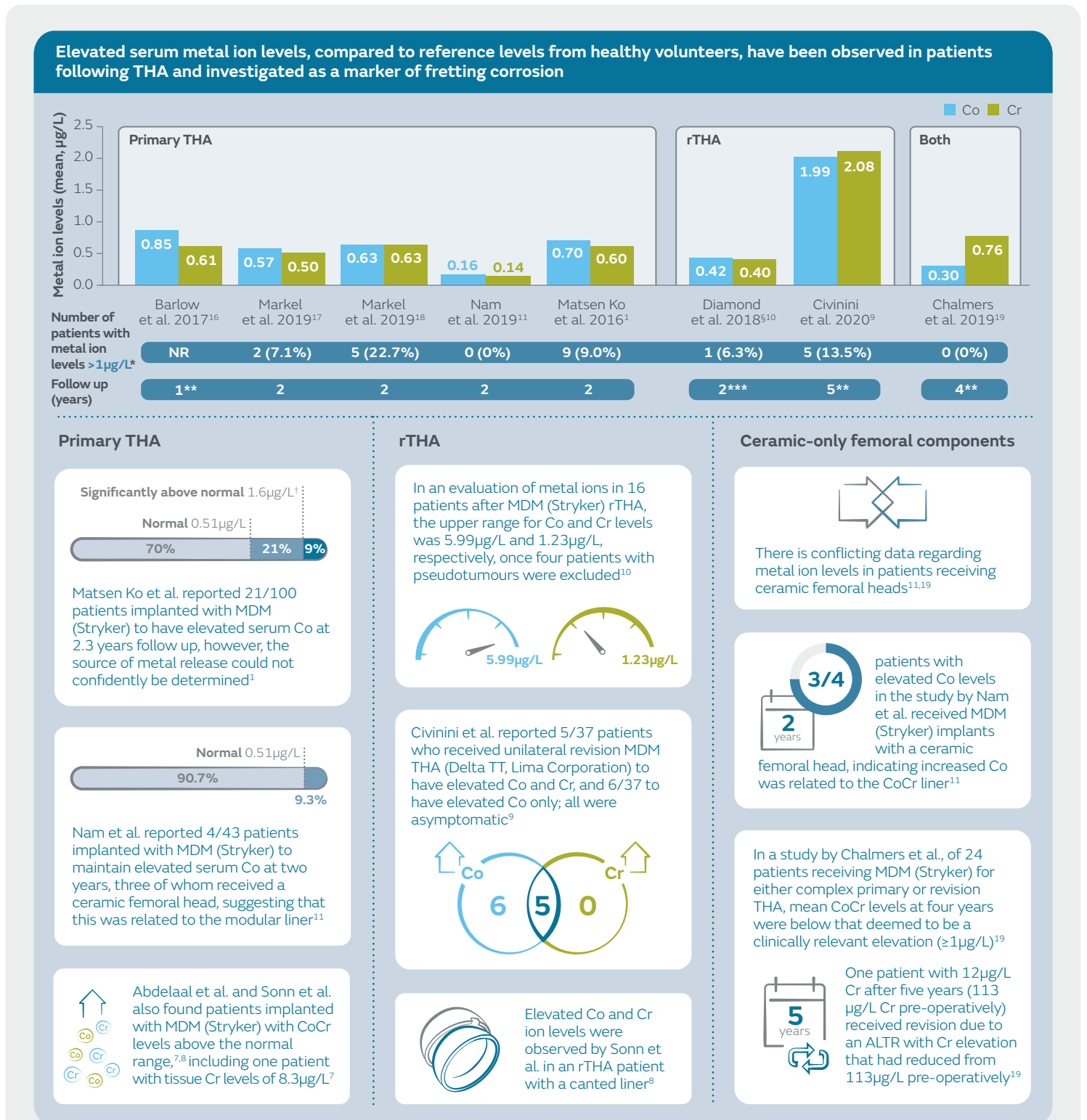


Figure 3. Evidence of elevated serum metal ion levels in patients who received MDM implants

*The clinical significance of serum metal ion levels >1µg/L is unclear.²⁰ **Mean follow up reported. ***Follow up not specified; minimum 2 years. [§]Median values reported. [†]Symptomatic patients with Co levels >1.6µg/L have previously been reported as requiring revision due to ALTR secondary to fretting corrosion.²¹ ALTR = adverse local tissue reaction, Co = cobalt, CoCr = cobalt-chromium, Cr = chromium, MDM = modular dual mobility, NR = not reported, rTHA = revision total hip arthroplasty, THA: total hip arthroplasty

+ Evidence in focus

Are metal ion elevations normal after THA?

The literature review identified one study that considered whether metal ion elevations are 'normal' after THA.¹⁶ The study investigated serum Co and Cr levels in 80 non-consecutive patients with well-functioning unilateral THA using a variety of bearing surfaces. No significant difference was found for serum Co and Cr levels between the four bearing surface groups (ceramic-on-ceramic [CoC], ceramic-on-polyethylene [CoP], metal-on-polyethylene [MoP] and MDM). However, a secondary analysis found patients with metal femoral heads (MoP, MDM [metal]) had significantly higher serum Co levels compared with those with ceramic heads (CoC, CoP, MDM [ceramic]): $1.05 \pm 1.25 \mu\text{g/L}$ vs $0.59 \pm 0.24 \mu\text{g/L}$; $p=0.0411$.

Whole blood analysis

Whole blood analysis has been used in studies of patients with MDM implants to investigate markers of inflammation and their association with elevated serum metal ions. Two studies from Markel et al. reported serum metal ion levels for patients with MDM implants with ceramic femoral heads at 2 years of follow up (Table 1).^{17,18}

Table 1. Pre- and postoperative serum metal ion levels for patients with mDM implants

	Metal ions	Preoperative	3 months	1 year	2 years	p-value
Study 1* ¹⁷ N=49	Co, $\mu\text{g/L}$ ($\pm\text{SD}$)	-	-	0.63 (0.32)	0.57 (0.20)	0.358
	Cr, $\mu\text{g/L}$ ($\pm\text{SD}$)	-	-	0.53 (0.16)	0.50 (0.00)	0.338
Study 2 ¹⁸ N=39 [‡]	Co, $\mu\text{g/L}$ ($\pm\text{SD}$)	0.51 (0.08)	0.85 (0.87)	0.64 (0.28)	0.63 (0.36)	0.045
	Cr, $\mu\text{g/L}$ ($\pm\text{SD}$)	0.53 (0.14)	0.58 (0.26)	0.56 (0.17)	0.63 (0.38)	0.496

*Statistical testing conducted between 1 and 2 years follow up; †One-way analysis of variance (ANOVA) used to determine statistically significant differences among mean values at the four time points. Paired Student's t-test showed the significant change in Co ($p<0.05$) was due to the increase at 3 months of follow up compared with preoperative level ($p<0.02$); ‡Preoperative, n=35; 3 months, n=30; 1 year, n=20; 2 years, n=22

Study 2 showed a statistically significant elevation in Co ion levels during the 2 year follow-up period compared to preoperative levels.¹⁸ However, there was no evidence in either study that an elevation in metal ion levels resulted in an immune response.

Circulating leukocyte profiles were stable and there was no observed increase in CD16+ monocyte levels, an important subpopulation of leukocytes that become elevated as part of the inflammatory response to antigens.^{17,18}

Caution should be taken when using the data based on metal ion analysis of blood/serum. While it is believed that elevated levels of Co or Cr ions in the circulatory system are an indicator of liner wear from MDM hips,¹ confirmatory evidence from a corresponding retrieved implant is not always available. Well-designed studies are required to investigate the link between elevated serum metal ion levels and fretting corrosion as well as to determine the clinical significance of the results.

Are canted liners a risk factor for fretting corrosion at the modular interface?

Romero et al. reported an incidence of malseating of the CoCr liner within the MDM Stryker implant of 5.8% (32/551).¹² *In vitro* modelling, which used current as a measure of fretting/corrosion, found that significantly less fretting/corrosion occurred for well-seated liners compared to malseated liners when peak loads greater than 2200N were applied ($p<0.05$). The onset fretting load, defined as the load at which there was marked increase (inflection point) in the fretting/corrosion current, was lower for canted liners than well-seated liners (2400 vs 2800N, respectively).¹² These loads are within the range expected during activities of daily living. Their results suggest that malseated liners may be at risk for fretting corrosion.¹²

Of the three cases reported by Sonn et al., all had evidence of fretting corrosion of the CoCr liner, with the liners of two MDM (Stryker) implants found to be canted upon revision surgery.⁸

The clinical consequences of malseating are unknown and further research is warranted.^{12,22}

Conclusions

- Implant retrieval has confirmed the occurrence of fretting corrosion of the CoCr liner of MDM implants²⁻⁸
- Elevated serum metal ions compared with reference levels from healthy volunteers have been reported in seven studies of patients with MDM implants, however, it is not always possible to determine the specific impact of the CoCr liner on this elevation due to other metal ion sources^{1,7-9,11,16,19}
- Canted liners may be at risk of fretting corrosion at the acetabular liner interface¹²
- Further studies are warranted to determine the extent to which the CoCr liner/titanium shell presents a fretting corrosion risk in MDM implants

Additional information

Table 2. Characteristics of studies reporting on MDM implant retrieval and serum metal ions

Author	Study design (single centre unless specified)	Primary or revision THA	n	Mean length of implantation (LOI)	Implant type	Femoral head
Abdelaal et al. 2021 ⁷	Retrospective, case study	Primary	1	96 months	MDM (Stryker)	CoCr (n=1)
Barlow et al. 2017 ¹⁶	Prospective case series	Primary	80 (20 MDM)	15 months	MDM (Stryker)	CoCr (n=10) Ceramic (n=10)
Chalmers et al. 2019 ¹⁹	Prospective cohort, noncomparative	Both	24	48 months	MDM (Stryker)	CoCr (n=0) Ceramic (n=24)
Civinini et al. 2020 ⁹	Cross-sectional study	Revision	37	61 months	Delta TT (Lima Corp)	CoCr (n=37) Ceramic (n=0)
Diamond et al. 2018 ¹⁰	Retrospective cohort, noncomparative	Revision	60 (16 for serum analysis)	39 months	MDM (Stryker)	CoCr (n=59) Ceramic (n=1)
Kolz et al. 2020 ⁶	Implant retrieval case series	Both	12	26 months	MDM (Stryker)	CoCr (n=8) Ceramic (n=4)
Lombardo et al. 2019 ⁵	Implant retrieval analysis	-	18 (10 MDM [Stryker])	13 months	MDM (Stryker) vs other hip systems	CoCr (n=8) Ceramic (n=2)
Markel et al. 2019 ¹⁷	Prospective cohort, noncomparative	Primary	49	24 months	MDM (Stryker)	CoCr (n=0) Ceramic (n=49)
Markel et al. 2019 ¹⁸	Prospective cohort, noncomparative	Primary	39	24 months	MDM (Stryker)	CoCr (n=0) Ceramic (n=39)
Matsen Ko et al. 2016 ¹	Retrospective cohort, noncomparative	Primary	100	28 months	MDM (Stryker)	CoCr (n=99) Ceramic (n=1)
Nam et al. 2019 ¹¹	Prospective cohort, noncomparative	Primary	43	24 months	MDM (Stryker)	CoCr (n=14) Ceramic (n=29)
Sonn et al. 2020 ⁸	Retrospective, case series	Both (2 primary; 1 revision)	3	42 months 48 months 48 months	MDM	CoCr (n=1) Ceramic (n=2)
Spece et al. 2018 ³	Implant retrieval case series	Both	29 (28 liners)	16 months	MDM (Stryker)	CoCr (n=25) Ceramic (n=4)
Sutter et al. 2017 ⁴	Retrospective, cohort, multicentre	Revision	64	38 months	MDM (Stryker)	
Tarity et al. 2017 ²	Implant retrieval analysis	Both	18	15 months	MDM (Stryker) vs MoM	CoCr (n=15) Ceramic (n=3)

References

1. Matsen Ko LJ, Pollag KE, Yoo JY, Sharkey PF. Serum metal ion levels following total hip arthroplasty with modular dual mobility components. *J Arthroplasty*. 2016;31(1):186–189.
 2. Tarity TD, Koch CN, Burket JC, Wright TM, Westrich GH. Fretting and corrosion at the backside of modular cobalt chromium acetabular inserts: a retrieval analysis. *J Arthroplasty*. 2017;32(3):1033–1039.
 3. Spece H, MacDonald DW, Mont MA, Lee G-C, Kurtz SM, Kurtz SM. Fretting corrosion and polyethylene damage mechanisms in modular dual mobility total hip arthroplasty. In: Mihalko W, Lemons J, Greenwald A, Kurtz S, eds. Beyond the implant: retrieval analysis methods for implant surveillance. *ASTM International*. 2018:106–117.
 4. Sutter EG, McClellan TR, Attarian DE, Bolognesi MP, Lachiewicz PF, Wellman SS. Outcomes of modular dual mobility acetabular components in revision total hip arthroplasty. *J Arthroplasty*. 2017;32(9):S220–S224.
 5. Lombardo DJ, Siljander MP, Gehrke CK, Moore DD, Karadshah MS, Baker EA. Fretting and corrosion damage of retrieved dual-mobility total hip arthroplasty systems. *J Arthroplasty*. 2019;34(6):1273–1278.
 6. Kolz JM, Wyles CC, Van Citters DW, Chapman RM, Trousedale RT, Berry DJ. In vivo corrosion of modular dual-mobility implants: a retrieval study. *J Arthroplasty*. 2020;35(11):3326–3329.
 7. Abdelaal MS, Zachwieja E, Sharkey PF. Severe corrosion of modular dual mobility acetabular components identified during revision total hip arthroplasty. Article. *Arthroplasty Today*. 2021;8:78–83.
 8. Sonn KA, Meneghini RM. Adverse local tissue reaction due to acetabular corrosion in modular dual-mobility constructs. *Arthroplasty Today*. 2020;6(4):976–980.
 9. Civinini R, Cozzi Lepri A, Carulli C, Matassi F, Villano M, Innocenti M. Patients following revision total hip arthroplasty with modular dual mobility components and cobalt-chromium inner metal head are at risk of increased serum metal ion levels. *J Arthroplasty*. 2020;35(6s):S294–S298.
 10. Diamond OJ, Konan S, Greidanus NV, Garbuz DS, Duncan CP, Masri BS. An early report of the use of a modular dual mobility articulation in revision acetabular reconstruction. *J Arthroplasty*. 2018;33(9):2961–2966.
 11. Nam D, Salih R, Nahhas CR, Barrack RL, Nunley RM. Is a modular dual mobility acetabulum a viable option for the young, active total hip arthroplasty patient? *Bone Joint J*. 2019;101-b(4):365–371.
 12. Romero J, Wach A, Silberberg S, et al. 2020 Otto Aufranc Award: Malseating of modular dual mobility liners: Incidence and implications. Conference Paper. *Bone Joint J*. 2020;102(7):20–26.
 13. De Martino I, Triantafyllopoulos GK, Sculco PK, Sculco TP. Dual mobility cups in total hip arthroplasty. *World J Orthop*. 2014;5(3):180–187.
 14. Hallab NJ, Jacobs JJ. Orthopedic Applications. In: Wagner WR, Sakiyama-Elbert SE, Zhang G, Yaszemski MJ, eds. *Biomaterials Science (Fourth Edition)*. Elsevier Academic Press; 2020:1079–1118.
 15. Smith+Nephew. Systematic literature review to identify the published evidence detailing the incidence of fretting corrosion of the CoCr liner of modular dual-mobility hip systems. 2021.
 16. Barlow BT, Ortiz PA, Boles JW, Lee Y-y, Padgett DE, Westrich GH. What Are normal metal ion levels after total hip arthroplasty? A serologic analysis of four bearing surfaces. *J Arthroplasty*. 2017;32(5):1535–1542.
 17. Markel D, Bou-Akl T, Rossi M, Pizzimenti NM, Wu B, Ren W-P. Response profiles of circulating leukocytes and metal ions in patients with a modular dual-mobility hip implant. *HIP International*. 2019;doi:10.1177/1120700019865530.
 18. Markel DC, Bou-Akl T, Rossi MD, Pizzimenti N, Wu B, Ren W. Blood metal levels, leucocyte profiles, and cytokine profiles in patients with a modular dual-mobility hip prosthesis. *Bone Joint J*. 2019;101-B(9):1035–1041.
 19. Chalmers BP, Mangold DG, Hanssen AD, Pagnano MW, Trousdale RT, Abdel MP. Uniformly low serum cobalt levels after modular dual-mobility total hip arthroplasties with ceramic heads. *Bone Joint J*. 2019;101-B(6, Suppl. B):57–61.
 20. Muñoz CS, Fernández-Martin JL, Marchante-Gayón JM, Alonso JIG, Cannata-Andía JB, Sanz-Medel A. Reference values for trace and ultratrace elements in human serum determined by double-focusing ICP-MS. *Journal article. Biol. Trace Elem. Res*. 2001;82(1):259–272.
 21. French JMR, Bramley P, Scattergood S, Sandiford NA. Adverse reaction to metal debris due to fretting corrosion between the acetabular components of modular dual-mobility constructs in total hip replacement: a systematic review and meta-analysis. *EFORT Open Rev*. 2021;6(5):343–353.
 22. Haddad FS. International dissemination. *Bone Joint J*. 2020;102-b(7):805–806.